



polymers



Article

Effects of Thermoforming on the Mechanical, Optical, Chemical, and Morphological Properties of PET-G: In Vitro Study

Edoardo Staderini, Giuseppe Chiusolo, Federica Guglielmi, Massimiliano Papi, Giordano Perini, Michele Tepedino and Patrizia Gallenzi

Special Issue

Advances in Shape Memory Polymeric Materials

Edited by

Dr. Yelena R. Sliozberg



<https://doi.org/10.3390/polym16020203>

Article

Effects of Thermoforming on the Mechanical, Optical, Chemical, and Morphological Properties of PET-G: In Vitro Study

Edoardo Staderini ^{1,2,†} , Giuseppe Chiusolo ^{1,†} , Federica Guglielmi ^{1,2,*} , Massimiliano Papi ^{3,4} ,
Giordano Perini ^{3,4} , Michele Tepedino ^{5,*}  and Patrizia Gallenzi ^{1,2}

- ¹ School of Dentistry, Dean: Prof. Massimo Cordaro, Catholic University of the Sacred Heart, IRCCS “A. Gemelli” University Polyclinic Foundation, Largo Agostino Gemelli 8, 00168 Rome, Italy; edoardo.staderini@unicatt.it (E.S.); giuseppechiusolo@libero.it (G.C.); patrizia.gallenzi@unicatt.it (P.G.)
- ² Postgraduate School of Orthodontics—Director: Prof. Massimo Cordaro, Catholic University of the Sacred Heart, Largo Agostino Gemelli 8, 00168 Rome, Italy
- ³ Department of Neurosciences, Catholic University of the Sacred Heart, Largo Francesco Vito 1, 00168 Rome, Italy; massimiliano.papi@unicatt.it (M.P.); giordano.perini@unicatt.it (G.P.)
- ⁴ IRCCS “A. Gemelli” University Polyclinic Foundation, Largo Agostino Gemelli 8, 00168 Rome, Italy
- ⁵ Department of Biotechnological and Applied Clinical Sciences, University of L’Aquila, Piazza Santa Margherita 2, 67100 L’Aquila, Italy
- * Correspondence: fe.guglielmi@gmail.com (F.G.); michele.tepedino@univaq.it (M.T.)
- † These authors contributed equally to this work.

Abstract: The effectiveness of clear aligners in correcting malocclusions is closely linked to the properties of the materials used to make them. The polymers used in the manufacture of clear aligners have well-established properties. However, the process of manufacturing clear aligners, known as thermoforming, involves thermal and mechanical shocks that may alter these properties. The objective of this study was to evaluate the effects of thermoforming on the mechanical, optical, chemical, and morphological properties of sixty PET-G specimens. The study compared the thickness, weight, absorbance, chemical structure, surface roughness, elastic modulus, yield strength, and breaking load of thirty thermoformed specimens with thirty non-thermoformed specimens. The study introduces a new approach by using standardized samples to analyze both chemical and physical properties. The results showed statistically significant differences in thickness (−15%), weight (−11%), and surface roughness (+1233% in roughness average; +1129% in RMS roughness) of the material. Additionally, a correlation was found between reduction in thickness and increase in opalescence. There was no significant change in the functionality of the aligners after thermoforming, as no significant mechanical changes were found. However, the increase in surface roughness may lead to plaque and fluid accumulation and worsen the fit of the aligners.

Keywords: thermoforming process; clear aligners; thermoplastic materials; glycol-modified polyethylene terephthalate; surface roughness



Citation: Staderini, E.; Chiusolo, G.; Guglielmi, F.; Papi, M.; Perini, G.; Tepedino, M.; Gallenzi, P. Effects of Thermoforming on the Mechanical, Optical, Chemical, and Morphological Properties of PET-G: In Vitro Study. *Polymers* **2024**, *16*, 203. <https://doi.org/10.3390/polym16020203>

Academic Editor: Yelena R. Sliozberg

Received: 4 November 2023

Revised: 30 December 2023

Accepted: 30 December 2023

Published: 10 January 2024



Copyright: © 2024 by the authors. Licensee MDPI, Basel, Switzerland. This article is an open access article distributed under the terms and conditions of the Creative Commons Attribution (CC BY) license (<https://creativecommons.org/licenses/by/4.0/>).

1. Introduction

Clear aligners are orthodontic devices made of thermoplastic material; based on clinical planning, they exert forces on the dental elements in the three planes of space [1,2]. The ability of clear aligners to move dental elements is closely related to the maintenance of the mechanical properties of the material from which they are made [3,4]. Several studies have shown that these mechanical properties are altered both by prolonged exposure to the intraoral environment and thermoforming [5–7]. Thermoforming is the process of heating a thermoplastic sheet to its softening point; this allows a clear aligner to be moulded by conforming the thermoplastic sheet to the crown surface of dental models [8,9].

In terms of morphological properties, Ryokawa et al. have shown how different materials used in the manufacture of orthodontic aligners undergo variations in thickness

after the thermoforming process; their study showed that the least stable materials were copolyesters (Essix A+) and polycarbonates (PC), with a reduction in thickness of 25.1% and 19.8%, respectively, while the most stable were polypropylene (PP) and glycol-modified polyethylene terephthalate (PET-G), with a reduction in thickness of 7.4% and 12.3%, respectively [10].

Regarding the optical and mechanical properties, Ryu et al. compared various materials with different thicknesses by evaluating the changes after thermoforming: PET-G specimens with a thickness of 1 mm suffered an about 2% reduction in transparency, an increase in water absorption of approximately $4 \mu\text{g}/\text{mm}^3$, and a decrease in the elastic modulus of about 160 Mpa [11]. Golkhani et al. also showed that the thermoforming process leads to a reduction in the elastic modulus, regardless of the type of material, as well as a reduction in the thickness of the specimens (0.1 mm reduction for PET-G) [12]. In contrast, Tamburrino et al. showed an 11% increase in the elastic modulus and a 9% increase in the yield strength of PET-G after thermoforming [13].

The heterogeneity of the results could be attributed to the influence of sample geometry on mechanical properties: Ryu et al. used trapezoidal prism-shaped samples, Golkhani et al. used rectangular sheets, Tamburrino et al. used “dumbbell-shaped” samples of polyethylene terephthalate (PET), glycol-modified polyethylene terephthalate (PET-G), and thermoplastic polyurethane (TPU); TPU has been shown to have higher weight variation but better elastic modulus stability than PET-G. Indeed, Elkholy et al. analysed the changes in the mechanical properties of PET-G samples with different geometries (stone model base plate, stone round disc, gable roof shaped specimen, stainless steel model holding plate) after thermoforming; they showed how the geometry of the material plays a crucial role in its ability to maintain mechanical properties [14]. Therefore, it is important to investigate the stability of mechanical properties using standardised specimens [15].

A deep understanding of thermoforming processes can assist clinicians in selecting the most suitable material and protocol for clear aligner therapy, without exerting excessive pressure on the periodontal ligament [16,17]. In addition, a thorough comprehension of the material's behaviour can enhance the accuracy levels of clear aligners, which currently range from 50 per cent to 73.6 per cent [18,19].

The aim of the present in vitro study is to analyse the impact of the thermoforming process on the mechanical, optical, chemical, and morphological properties of standardised PET-G “dumbbell-shaped” samples.

The novelty of this study concerns the integration of both chemical and mechanical testing procedures, while most studies in the literature analysed only either chemical or physical properties [15–17]. Additionally, all these assessments were conducted on ISO samples. Furthermore, the study concentrated on detecting the morphological variations of the material concerning surface roughness, which has been scarcely investigated in the literature thus far. In fact, the thermal shock associated with the thermoforming process could alter the surface roughness and thus partially affect the optical and absorption properties of the material [20,21]. Lira et al. found an increase in surface roughness after 14 days of intraoral use, resulting in a loss of transparency and increased pigmentation of the aligners [22]. However, no study has yet investigated the effects of thermoforming on surface roughness [21,23].

2. Materials and Methods

At baseline, 60 PET-G sheets (Erkodur, Erkodent Erich Kopp GmbH, Pfalzgrafenweiler, Germany) were selected and randomly assigned by a third person (not involved in the research) to two different groups: 30 sheets (thermoforming group—TG) underwent the thermoforming process, while 30 sheets (control group—CG) were analysed as supplied.

The thermoforming process was carried out using a Ministar S machine (Ministar S, Scheu, Iserlohn, Germany) according to the manufacturer's recommendations for pressure, heating time, and cooling time. Specifically, a pressure of 4/4.2 bar, a temperature of $175 \pm 10^\circ$, a heating time of 28'', and a cooling time of 30'' were applied. The disk tempera-

ture was measured at the surface using a laser thermometer (Fluke 62 Max +, Fluke, Everett, Washington, DC, USA). Every PET-G sheet was vacuum thermoformed without the use of any mould to simulate the stress of the thermoforming procedure. From each PET-G sheet, “dumbbell-shaped” specimens were cut using a laser cutting machine (BCL1309X, Bodor, Jinan, China) (Figure 1).

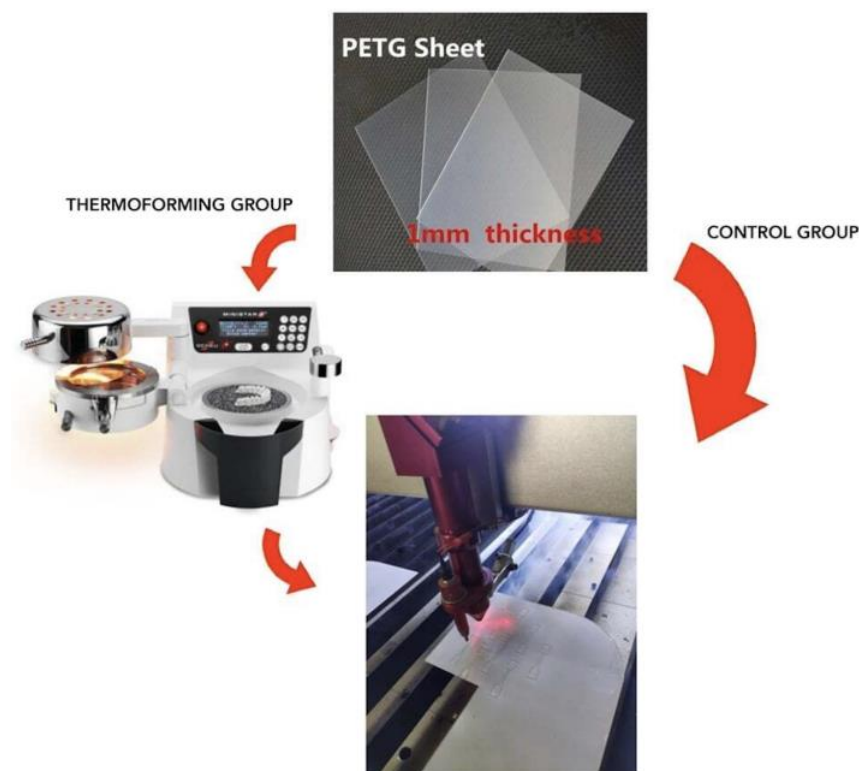


Figure 1. CG and TG sample making process.

The shape, size, and thickness of the “dumbbell-shaped” specimens followed the EN ISO 527-2 guidelines for type 5B specimens. To ensure consistency in mechanical and optical measurements, stringent experimental protocols were adhered to throughout the testing process.

The morphology of the specimens consists of two shoulders (at the ends) and a gauge section (in the middle). The shoulders are wider than the gauge section, resulting in a stress concentration in the middle when the sample is subjected to a tensile load. In physics, if a specimen fails in the middle section, it is due to the material reaching its maximum tensile strength; if, on the other hand, the specimen fails at one end or in the socket itself, the failure can be attributed to improper loading or a pre-existing defect in the material. The “dumbbell-shaped” morphology is therefore designed to increase the probability of specimen failure at maximum tensile load.

Thickness analysis, weight analysis, absorbance analysis, Fourier-transform infrared spectroscopy (FTIR), surface roughness analysis, and tensile tests were evaluated (Table 1).

Table 1. Properties analysed and tests performed.

Properties	Test
Morphological properties	Thickness; weight; surface roughness
Optical properties	Absorbance
Chemical properties	Fourier-transform infrared spectroscopy (FTIR)
Mechanical properties	Tensile tests

2.1. Thickness

The thickness of the specimens was measured with a digital electronic gauge (Fervi SpA, Vignola, Italy), with an accuracy of 0.01 mm. Measurements were taken at random points on the shoulders and in the gauge section, and then the mean was calculated.

2.2. Weight

Weight was measured using an Entris scale (Entris, Sartorius, Germany) with a readability of 0.1 mg.

2.3. Absorbance

Absorbance was measured in the visible light spectrum (frequency range: 230–700 nm; step: 5 nm) through a Cytation3 spectrophotometer (Cytation3 Imaging reader, Biotek, Santa Clara, CA, USA) (Figure S1a). This measurement was performed to assess any changes in the transparency of the material after thermoforming. Each specimen was fixed to a customized thermoplastic holder (Polylactic Acid PLA, FILOALFA[®], Torino, Italy) (Figure S1b,c), and then inserted into a plate (*take 3*) of the machine. The above-mentioned holder was realized using a 3D printer (Crealty Ender-3, Longhua Dist., Shenzhen, China). After the measurement, the data were transferred from the machine to specific software (Gen 5, Microplate Reader and Imager Software, Biotek, Santa Clara, CA, USA) capable of collecting and analysing them. All measurements were performed at a constant temperature of 23 °C.

2.4. FTIR Spectroscopy

This FTIR spectroscopy was carried out to investigate any changes in the chemical composition of the PET-G material after the thermoforming process. The measurements were carried out using the Alpha II spectrometer (Alpha II, Bruker, Germany) (Figure S2a), which is able to detect the absorbance of the samples and to compare the spectrum of the results obtained with an internal software. This test aimed to evaluate whether the thermoforming process leads to changes in the arrangement and distribution of the chemical bonds of the polymer under analysis. Spectral transmittance data were obtained with a frequency range (MIR) of 4000–600 cm⁻¹; 24 consecutive scans were performed for each measurement. All measurements were made on one shoulder of the sample as the chemical composition of the material is expected to be the same at each point in the sample.

2.5. Surface Roughness

Surface roughness was assessed using an atomic force microscope (JPK Nanowizard II, Bruker, Germany) (Figure S2b). The surface roughness parameters recorded were (a) *Ra* (roughness average), the arithmetic average of the absolute values of the profile heights over the evaluation length, and (b) *Rq* (RMS roughness), the root mean square (RMS) average of the profile heights over the evaluation length. Measurements were randomly taken at multiple sample points and then the mean was calculated.

2.6. Tensile Tests

Tensile tests were carried out with a Univert machine (Univert, Cell Scale, Waterloo, ON, Canada) in accordance with EN ISO 527-1:2019 (Figure S3a,b). The Univert machine allowed for evaluation of the tensile strength of the materials by means of two parameters: the displacement of the two clamps per unit of time, or the force between the two clamps per unit of time. In accordance with the literature, the first setting was chosen for this study, as it allowed for evaluation of the force required to achieve a given effect on the material. Two different strain rates were used: the slow dynamic (0.8 mm/s) allowed us to analyse the yield strength; the fast dynamic (8 mm/s) allowed us to analyse the breaking load and the elastic modulus (Young's modulus).

2.7. Statistical Analysis

All data are expressed as mean \pm standard deviation.

Dalaie et al. have shown that a sample size of 5 specimens was required to obtain a power of the study equivalent to 0.8, considering an α error of 0.05 [6]. In this experimental study, both non-destructive and destructive tests were performed. A total of 30 samples were selected for non-destructive testing (thickness, weight, absorbance, FTIR spectroscopy, surface roughness). Instead, the analysis of the mechanical properties consisted of destructive testing; therefore, 15 specimens were employed for the measurement of the yield strength and 15 for the measurement of the breaking load and the elastic modulus. Independent *t*-tests were performed for the synchronous comparison of the material before and after the thermoforming process. The inter-operator reproducibility of the results has been systematically verified by conducting *t*-tests on a cohort of 30 samples. All the procedures were meticulously controlled and repeated by one researcher (M.P.) to validate the intra-operator reliability and replicability of the obtained outcomes. The significance level was set at $p < 0.01$. All data were analysed using Systat software (version 8.0, SYSTAT Software Inc. (SSI), San Jose, CA, USA).

3. Results

3.1. Reliability

The paired *t*-test confirmed the intra- and inter-operator reproducibility of the observed effects across the sample set.

3.2. Thickness

As shown in Table 2, the thermoforming process resulted in a 15% reduction in the thickness of the specimens ($p < 0.01$); the height of the specimens remained unchanged.

Table 2. Mean values and standard deviations of thickness and height of control group (CG) and thermoforming group samples (TG).

	CG	TG
Thickness (mm)	0.99 (± 0.03)	0.84 (± 0.01)
Height (mm)	1.84 (± 0.02)	1.84 (± 0.01)

3.3. Weight

As shown in Figure 2 and Table 3, the average weight of the samples was reduced by approximately 11% after thermoforming ($p < 0.01$).

Table 3. Mean values and standard deviations of weight of CG and TG samples.

	CG	TG
Average weight (g)	4.313 (± 0.001)	3.859 (± 0.001)

3.4. Absorbance

As shown in Figure 3, no significant differences in the optical density of the TG samples could be detected as the absorbance spectra overlapped. According to the Beer–Lambert law, light attenuation depends on the properties of the material through which the light is passing:

$$A = \epsilon \ell$$

where:

A is the absorbance.

ϵ is the molar attenuation coefficient or absorptivity of the attenuating species.

ℓ is the optical path length in cm (thickness).

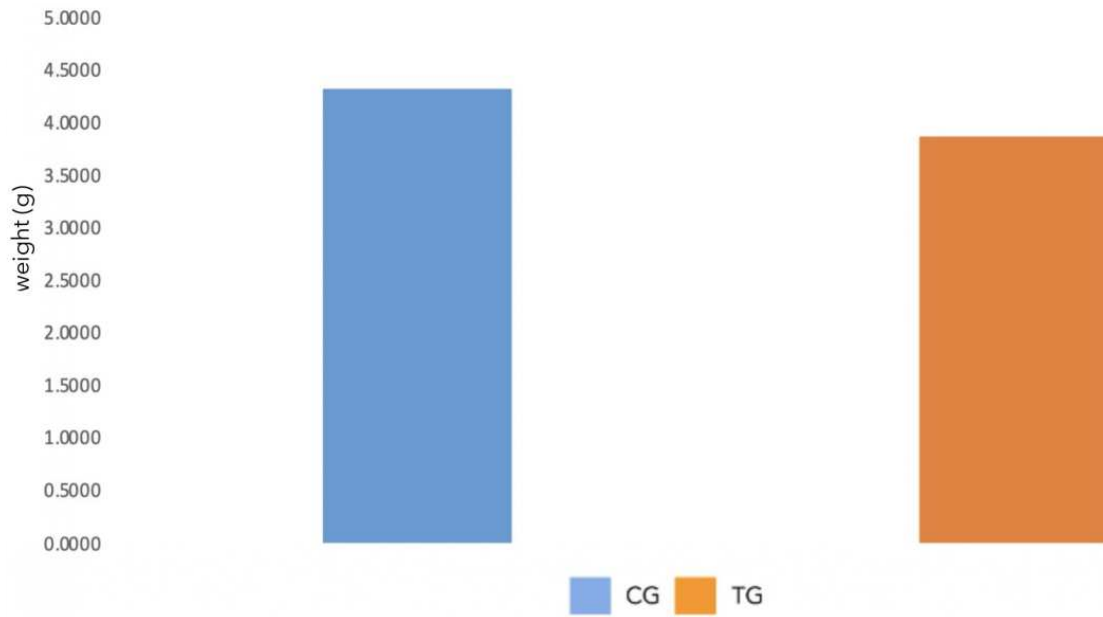


Figure 2. Average weight of the CG (blue) and TG (orange) samples.

Since the absorbance values were similar between CG and TG specimens, but the thickness of the TG specimens was reduced after thermoforming, we should expect that there was an inversely proportional increase in the molar attenuation coefficient.

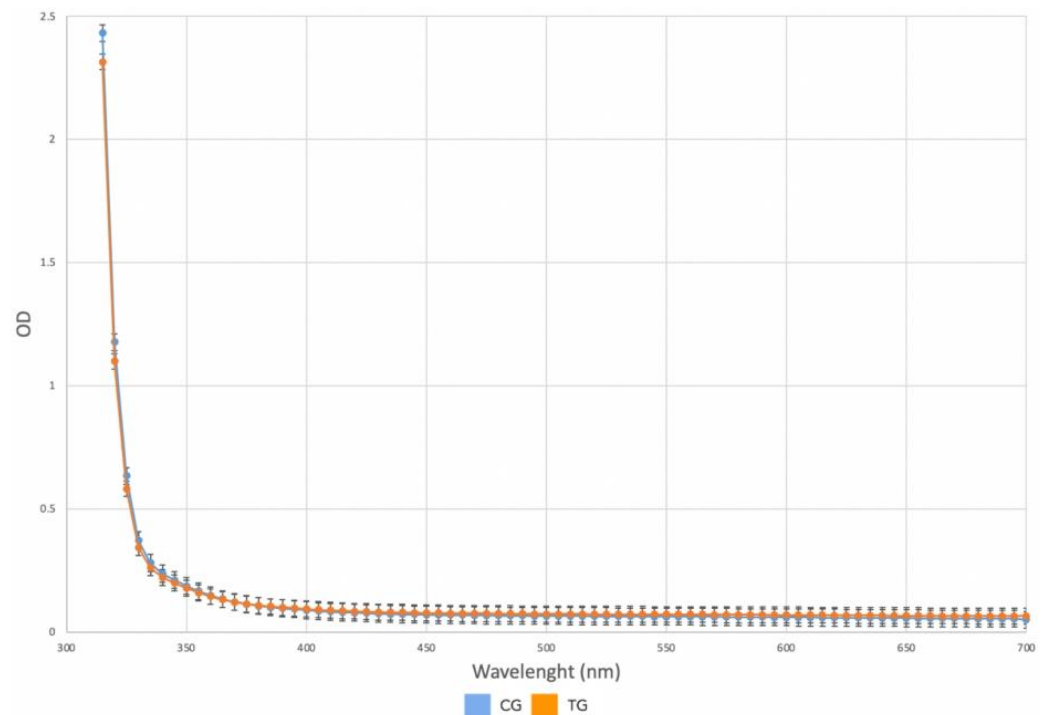


Figure 3. Absorbance spectra of the CG and TG samples; average absorbance CG (blue); average absorbance TG (orange).

3.5. FTIR Spectroscopy

As shown in Figure 4, there were no significant chemical changes in the samples after treatment.

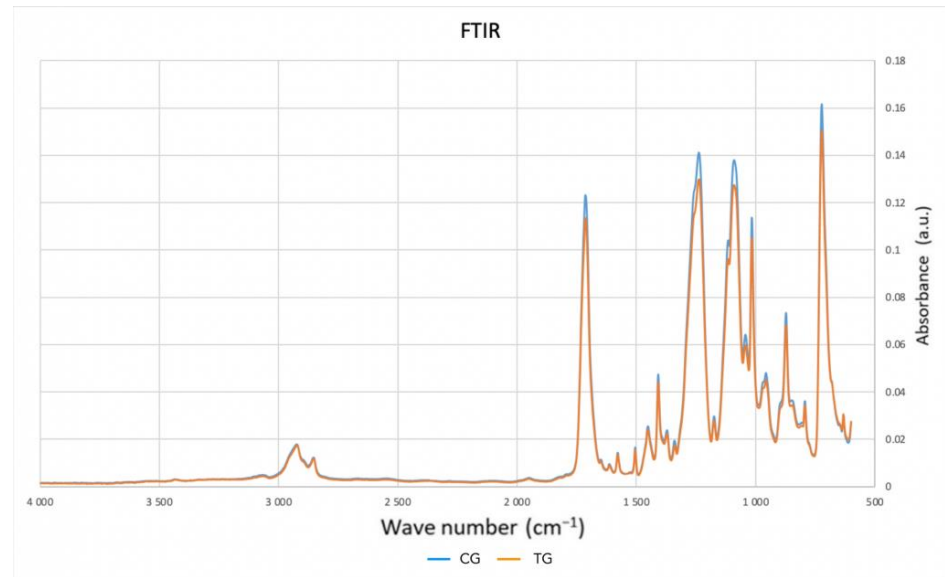


Figure 4. Average FTIR spectroscopy spectrum of the CG (blue) and TG (orange) samples.

3.6. Surface Roughness

As shown in Figure 5a,b, the material underwent important alterations in surface roughness after thermoforming.

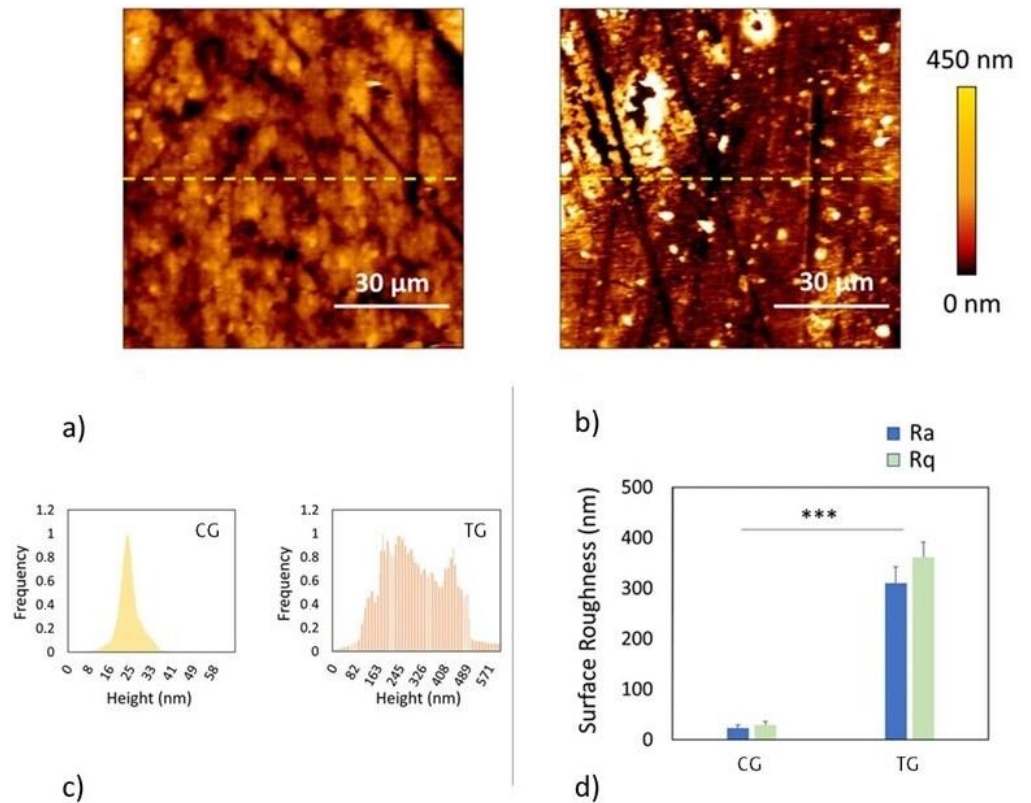


Figure 5. (a) Representative surface of the CG sample made with the atomic force microscope; (b) representative surface of the TG sample made with the atomic force microscope; (c) histogram chart of the profile heights on the surface of a CG sample and a TG sample. “Frequency” refers to how often a given value was observed. The curve is normalized to 1, meaning that the most frequent value is assigned a value of 1 and all other values are proportional; (d) quantification of CG and TG roughness based on roughness average (R_a) and RMS roughness (R_q). * $p < 0.01$; ** $p < 0.001$; *** $p < 0.0001$.

As shown in Figure 5c,d and in Table 4, the thermoforming process resulted in an increase of approximately 1233% in the roughness average, which is the arithmetic average of the absolute values of the profile heights over the evaluation length, and an increase of approximately 1129% in the RMS roughness, which is the root mean square average of the profile heights over the evaluation length.

Table 4. Mean values and standard deviations of roughness average (R_a) and RMS roughness (R_q) of CG and TG samples.

	CG	TG
Roughness average (R_a)	23.28 (± 6.145)	310.34 (± 31.626)
RMS roughness (R_q)	29.38 (± 7.067)	361.16 (± 30.656)

3.7. Tensile Tests

As shown in Table 5, no statistically significant differences in mechanical properties between CG and TG samples were appreciated ($p > 0.01$). TG samples were found to have inferior mechanical properties solely due to the variation in thickness.

Table 5. Mean values and standard deviations of yield point, Young's modulus, and breaking load of CG and TG samples.

	CG	TG
Yield point (MPa)	41.3 (± 3.8)	42.3 (± 1.8)
Young's modulus (GPa)	0.73 (± 0.01)	0.72 (± 0.01)
Breaking load (MPa)	47.4 (± 1.1)	48.5 (± 2.1)

Both groups (CG and TG) showed the same mechanical behaviours under destructive tensile tests. The fast dynamics showed that the breakage of the molecular bonds of the polymer sample occurred after about 6% of elongation (Figure 6a). With the slow dynamics, it was not possible to observe the breakage of the molecular bonds of the polymer but only a slow elongation of its fibres (Figure 6b).

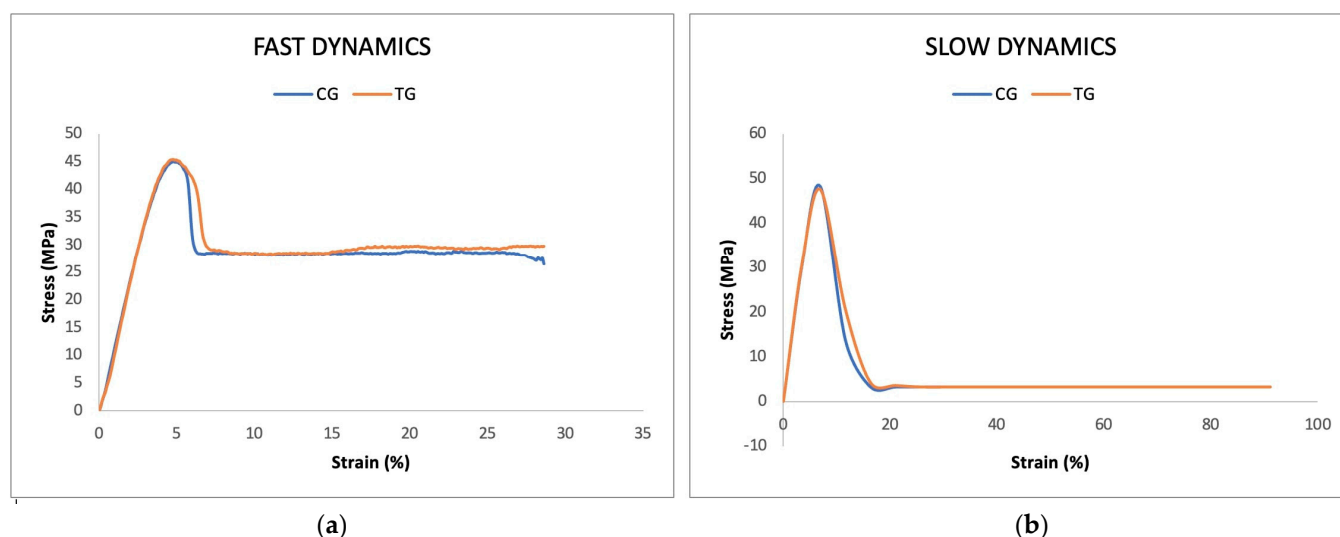


Figure 6. (a) Fast dynamics: representative stress–strain curve (8 mm/s) of the CG (blue) and TG (orange) samples; (b) slow dynamics: representative stress–strain curve (0.8 mm/s) of the CG (blue) and TG (orange) samples.

4. Discussion

4.1. Interpretation of the Results in the Context of the Available Literature

In this experimental study, the mechanical, chemical, optical, and morphological properties of PET-G, one of the most used materials for clear aligners, were analysed. Several studies in the literature have attempted to evaluate whether this process could lead to significant alterations in the material's properties, as it is known that the maintenance of its properties is fundamental to keep its ability to move teeth [24,25].

Dalaie et al. showed that thermoforming significantly ($p < 0.01$) reduced the flexural modulus, hardness, elastic modulus, and glass transition temperature of PET-G sheets (Erkodur, Erkodent Erich Kopp GmbH, Pfalzgrafenweiler, Germany) [6]. Golkhani et al. also analysed the variations in PET-G sheets following the thermoforming process and found a statistically significant reduction in both elastic modulus (557 MPa, from 2746 to 2189 MPa) and thickness (0.10 mm) [12]. Similarly, Ryu et al. also observed a significant reduction in thickness of PET-G trapezoidal prism specimens ($p < 0.01$) [11].

Although the present study involved the use of standardised “dumbbell-shaped” specimens, our results are consistent with those of Golkhani et al. and Ryu et al., as the specimens underwent a significant average thickness reduction of 0.15 mm ($p < 0.01$) after thermoforming. These results agree with a study by Palone et al., who used 2D methods to assess the thickness variation of different types of aligners after thermoforming: they showed that regardless of the material, thermoforming significantly reduces thickness of the aligners [16,26].

This reduction in thickness could be the main cause of the subtle changes in the mechanical properties of the material [11,12,27]. Indeed, there was a slight reduction in the elastic modulus of the material, although this reduction was not significant ($p > 0.01$), while the studies by Dalaie et al. and Golkhani et al. on PET-G sheets showed a significant reduction [6,12].

In contrast to the present data, Tamburrino et al. showed a significant increase in the elastic modulus of dumbbell-shaped specimens after thermoforming ($p < 0.05$), and they attributed this increase to a process known as “drawing”, which occurs when the material is heated and stretched: the polymer chains slide over each other, thus orienting part of the chains along the direction of the force [13].

As a possible explanation for the conflicting data on the variation of elastic modulus after thermoforming, FTIR analysis showed that the thermoforming process did not change the polymeric structure of the specimens. In physics, the elastic modulus of a sample would be expected to change if any variation occurred in the crystalline/amorphous ratio of the polymer structure. In this case, there were no statistically significant differences in the elastic modulus of the TG and CG group, as expected.

When analysing stress–strain curves, it is important to note the impact of pulling speed on the polymer's mechanical behaviour. Our data shows that both groups (CG and TG) exhibit similar mechanical behaviours during destructive tensile tests. However, fast dynamics reveal that the polymer sample's molecular bonds break after approximately 6% elongation. In contrast, slow dynamics only allow for the observation of a slow elongation of the polymer fibres, without the possibility of observing the rupture of molecular bonds. These findings emphasize the critical role of the rate of force application in determining the mechanical properties of the polymer [28,29]. Rapid breakage indicates increased material brittleness, suggesting that the rupture process occurs abruptly when subjected to high stresses. On the other hand, slow pulling results in a more gradual deformation, highlighting the influence of pulling speed on the polymer's mechanical response under tensile stress. This nuanced understanding enhances the characterization of the polymer's mechanical properties, illuminating its behaviour under various loading conditions and offering valuable insights for practical applications and material design considerations.

Regarding the optical properties, this study showed that the reduction in thickness as well as the increase in surface roughness may have indirectly played a role in increasing the optical density of the samples.

In fact, the analysis of the surface roughness of the specimens showed very interesting data: the average roughness and the RMS roughness increased by about 1233% and 1129%, respectively, after thermoforming (Figure 5c). This increase in surface roughness could explain the discrepancy between mass and thickness reduction (10% and 15%, respectively) and could also be at the basis of the differences in absorbance between CG and TG specimens.

In our opinion, increased surface roughness, combined with a lack of proper oral hygiene, may have detrimental effects on plaque retention and the absorption of water, saliva, and other fluids, leading to discoloration of clear aligners during intraoral use [21,22].

However, further investigation is required to determine the clinical consequences of surface roughness alterations in the physiological process of fluid and debris absorption, as well as plaque accumulation [30,31].

As for the chemical properties, however, these do not appear to be altered by the thermoforming process.

4.2. Strengths of the Study

This study was carried out on samples that followed the European ISO guidelines for thermoplastic samples. Moreover, all tests were performed on 30 specimens, except for mechanical measurements which were performed on 15 specimens. Previous studies by Ryu et al. and Dalaie et al. performed sample size analysis enrolling 4 and 5 samples, respectively [6,11]. Since our study showed conflicting data on elastic modulus with those provided by Dalaie et al., it was chosen to increase the sample size by approximately 150% to enhance the study's statistical power [6].

4.3. Limitations of the Study

A limitation of this study could be related to the fact that all the tests were carried out exclusively on "dumbbell-shaped" samples and not on the aligners themselves; however, the shape of the aligners is not homogeneous as they adapt to the shape of the patient's arch form, thus hampering the reproducibility of the data.

There are only a few studies in the literature that used aligners as samples for the evaluation of optical properties [7,32]. An in-house pilot analysis (data not shown) revealed that using aligners as specimens could lead to unpredictable results, especially for mechanical and optical tests.

5. Conclusions

The present in vitro study aimed to assess the mechanical, optical, chemical, and morphological properties of PET-G dumbbell-shaped specimens after the thermoforming process. The novelty of this study resides on the comprehensive analysis of both chemical and mechanical testing procedures, combined with the use of ISO samples, and the analysis of surface roughness. The research methodology investigated the surface roughness, as it plays a critical role both for optical and absorption properties of aligner materials.

The findings of the present study can be summarized as follows:

- (a) Morphological changes: the thickness of the TG specimens was reduced by 15% and the molecular weight by 11%; the surface roughness showed a statistically significant increase.
- (b) Optical changes: the material seemed to be more opaque, probably due to the surface roughness increase that occurs after thermoforming.
- (c) There were no chemical changes in the material.
- (d) The mechanical properties of the PET-G dumbbell-shaped specimens remain almost unchanged after thermoforming; the slight differences in mechanical behaviour seem to be related to the thickness reduction of the specimens after thermoforming.

These findings suggest that the mechanical properties of PET-G material, and consequently the clinical performance of the aligners, appear to remain stable after thermoforming. However, the thermoforming process altered the morphological (molecular weight,

thickness, and surface roughness) and optical properties (light absorbance) of PET-G material, thus affecting the aesthetics of clear aligners. Future studies should investigate the clinical consequences of the increase in surface roughness. It may also be important to assess whether overcorrection of the initial material thickness is necessary to compensate for the reduction that occurs after thermoforming.

Supplementary Materials: The following supporting information can be downloaded at: <https://www.mdpi.com/article/10.3390/polym16020203/s1>, Figure S1. (a) Spectrophotometer Cytation 3; (b) 3D printed customized support to fix the samples in the plate; (c) “dumbbell-shaped” sample fixed in the customized plate. Figure S2. (a) Alpha II spectrometer; (b) Atomic force microscope. Figure S3. (a) Univert–CellScale; (b) tensile test with clamps.

Author Contributions: Conceptualisation, E.S. and G.C.; methodology, E.S. and M.P.; software, M.P.; validation, M.P. and P.G.; formal analysis, M.P.; investigation, E.S., G.C. and F.G.; resources, M.T.; data curation, G.P.; writing—original draft preparation, E.S. and G.C.; writing—review and editing, G.C.; visualisation, M.T.; supervision, P.G. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Institutional Review Board Statement: Not applicable.

Data Availability Statement: The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

Acknowledgments: We would like to acknowledge the contribution of 3D Bioprinting Research Core Facility G-STeP of the Fondazione Policlinico Universitario “A. Gemelli” IRCCS, and Alberto Augello for sample processing. We would like to thank Nuvola® (Biomax Spa, 36100, Vicenza, Italy) for the study material and the financial support.

Conflicts of Interest: The authors declare no conflicts of interest.

References

1. Rossini, G.; Parrini, S.; Castroflorio, T.; Deregibus, A.; Debernardi, C.L. Efficacy of clear aligners in controlling orthodontic tooth movement: A systematic review. *Angle Orthod.* **2015**, *85*, 881–889. [[CrossRef](#)] [[PubMed](#)]
2. Weir, T. Clear aligners in orthodontic treatment. *Aust. Dent. J.* **2017**, *62* (Suppl. S1), 58–62. [[CrossRef](#)] [[PubMed](#)]
3. Fang, D.; Zhang, N.; Chen, H.; Bai, Y. Dynamic stress relaxation of orthodontic thermoplastic materials in a simulated oral environment. *Dent. Mater. J.* **2013**, *32*, 946–951. [[CrossRef](#)] [[PubMed](#)]
4. Kohda, N.; Iijima, M.; Muguruma, T.; Brantley, W.A.; Ahluwalia, K.S.; Mizoguchi, I. Effects of mechanical properties of thermoplastic materials on the initial force of thermoplastic appliances. *Angle Orthod.* **2013**, *83*, 476–483. [[CrossRef](#)] [[PubMed](#)]
5. Bucci, R.; Rongo, R.; Levate, C.; Michelotti, A.; Barone, S.; Razionale, A.V.; D’Anto, V. Thickness of orthodontic clear aligners after thermoforming and after 10 days of intraoral exposure: A prospective clinical study. *Prog. Orthod.* **2019**, *20*, 36. [[CrossRef](#)] [[PubMed](#)]
6. Dalaie, K.; Fatemi, S.M.; Ghaffari, S. Dynamic mechanical and thermal properties of clear aligners after thermoforming and aging. *Prog. Orthod.* **2021**, *22*, 15. [[CrossRef](#)] [[PubMed](#)]
7. Lombardo, L.; Arreghini, A.; Maccarrone, R.; Bianchi, A.; Scalia, S.; Siciliani, G. Optical properties of orthodontic aligners—spectrophotometry analysis of three types before and after aging. *Prog. Orthod.* **2015**, *16*, 41. [[CrossRef](#)]
8. Leite, W.O.; Campos Rubio, J.C.; Mata Cabrera, F.; Carrasco, A.; Hanafi, I. Vacuum Thermoforming Process: An Approach to Modeling and Optimization Using Artificial Neural Networks. *Polymers* **2018**, *10*, 143. [[CrossRef](#)]
9. Tartaglia, G.M.; Mapelli, A.; Maspero, C.; Santaniello, T.; Serafin, M.; Farronato, M.; Caprioglio, A. Direct 3D Printing of Clear Orthodontic Aligners: Current State and Future Possibilities. *Materials* **2021**, *14*, 1799. [[CrossRef](#)]
10. Ryokawa, H.; Miyazaki, Y.; Fujishima, A.; Miyazaki, T.; Maki, K. The mechanical properties of dental thermoplastic materials in a simulated intraoral environment. *Orthod. Waves* **2006**, *65*, 64–72. [[CrossRef](#)]
11. Ryu, J.H.; Kwon, J.S.; Jiang, H.B.; Cha, J.Y.; Kim, K.M. Effects of thermoforming on the physical and mechanical properties of thermoplastic materials for transparent orthodontic aligners. *Korean J. Orthod.* **2018**, *48*, 316–325. [[CrossRef](#)]
12. Golkhani, B.; Weber, A.; Keilig, L.; Reimann, S.; Bourauel, C. Variation of the modulus of elasticity of aligner foil sheet materials due to thermoforming. *J. Orofac. Orthop. = Fortschritte Kieferorthopädie Organ/Off. J. Dtsch. Ges. Kieferorthopädie* **2022**, *83*, 233–243. [[CrossRef](#)]
13. Tamburrino, F.; D’Anto, V.; Bucci, R.; Alessandri-Bonetti, G.; Barone, S.; Razionale, A.V. Mechanical Properties of Thermoplastic Polymers for Aligner Manufacturing: In Vitro Study. *Dent. J.* **2020**, *8*, 47. [[CrossRef](#)] [[PubMed](#)]

14. Elkholly, F.; Schmidt, S.; Amirkhani, M.; Schmidt, F.; Lapatki, B.G. Mechanical Characterization of Thermoplastic Aligner Materials: Recommendations for Test Parameter Standardization. *J. Healthc. Eng.* **2019**, *2019*, 8074827. [[CrossRef](#)] [[PubMed](#)]
15. Ciavarella, D.; Tepedino, M.; Gallo, C.; Montaruli, G.; Zhurakivska, K.; Coppola, L.; Troiano, G.; Chimenti, C.; Laurenziello, M.; Lo Russo, L. Post-orthodontic position of lower incisors and gingival recession: A retrospective study. *J. Clin. Exp. Dent.* **2017**, *9*, e1425–e1430. [[CrossRef](#)] [[PubMed](#)]
16. Palone, M.; Longo, M.; Arveda, N.; Nacucchi, M.; Pascalis, F.; Spedicato, G.A.; Siciliani, G.; Lombardo, L. Micro-computed tomography evaluation of general trends in aligner thickness and gap width after thermoforming procedures involving six commercial clear aligners: An in vitro study. *Korean J. Orthod.* **2021**, *51*, 135–141. [[CrossRef](#)] [[PubMed](#)]
17. Tepedino, M.; Iancu-Potrubacz, M.; Ciavarella, D.; Masedu, F.; Marchione, L.; Chimenti, C. Expansion of permanent first molars with rapid maxillary expansion appliance anchored on primary second molars. *J. Clin. Exp. Dent.* **2018**, *10*, e241–e247. [[CrossRef](#)]
18. Haouili, N.; Kravitz, N.D.; Vaid, N.R.; Ferguson, D.J.; Makki, L. Has Invisalign improved? A prospective follow-up study on the efficacy of tooth movement with Invisalign. *Am. J. Orthod. Dentofac. Orthop. Off. Publ. Am. Assoc. Orthod. Its Const. Soc. Am. Board Orthod.* **2020**, *158*, 420–425. [[CrossRef](#)]
19. Lombardo, L.; Arreghini, A.; Ramina, F.; Huanca Ghislanzoni, L.T.; Siciliani, G. Predictability of orthodontic movement with orthodontic aligners: A retrospective study. *Prog. Orthod.* **2017**, *18*, 35. [[CrossRef](#)]
20. Zhong, N.; Zhu, X.; Liao, Q.; Wang, Y.; Chen, R.; Sun, Y. Effects of surface roughness on optical properties and sensitivity of fiber-optic evanescent wave sensors. *Appl. Opt.* **2013**, *52*, 3937–3945. [[CrossRef](#)]
21. Eslami, S.; Kopp, S.; Goteni, M.; Dahmer, I.; Sayahpour, B. Alterations in the surface roughness and porosity parameters of directly printed and Invisalign aligners after 1 week of intraoral usage: An in vivo prospective investigation. *Am. J. Orthod. Dentofac. Orthop. Off. Publ. Am. Assoc. Orthod. Its Const. Soc. Am. Board Orthod.* **2023**, *165*, 73–79. [[CrossRef](#)]
22. Lira, L.F.; Vargas, E.O.A.; da Silva, E.M.; da Silva Meirelles Dória Maia, J.N.; Elzubair, A.; de Moraes, L.S.; de Souza Camargo, S.A., Jr.; Serra, G.; de Souza, M.M.G. Effect of oral exposure on chemical, physical, mechanical, and morphologic properties of clear orthodontic aligners. *Am. J. Orthod. Dentofac. Orthop. Off. Publ. Am. Assoc. Orthod. Its Const. Soc. Am. Board Orthod.* **2023**, *164*, e51–e63. [[CrossRef](#)]
23. Di Carlo, G.; Zara, F.; Rocchetti, M.; Venturini, A.; Ortiz-Ruiz, A.J.; Luzzi, V.; Cattaneo, P.M.; Polimeni, A.; Voza, I. Prevalence of Sleep-Disordered Breathing in Children Referring for First Dental Examination. A Multicenter Cross-Sectional Study Using Pediatric Sleep Questionnaire. *Int. J. Environ. Res. Public Health* **2020**, *17*, 8460. [[CrossRef](#)] [[PubMed](#)]
24. Hahn, W.; Dathe, H.; Fialka-Fricke, J.; Fricke-Zech, S.; Zapf, A.; Kubein-Meesenburg, D.; Sadat-Khonsari, R. Influence of thermoplastic appliance thickness on the magnitude of force delivered to a maxillary central incisor during tipping. *Am. J. Orthod. Dentofac. Orthop. Off. Publ. Am. Assoc. Orthod. Its Const. Soc. Am. Board Orthod.* **2009**, *136*, 12.e1–12.e7; discussion 12–13. [[CrossRef](#)] [[PubMed](#)]
25. Hahn, W.; Fialka-Fricke, J.; Dathe, H.; Fricke-Zech, S.; Zapf, A.; Gruber, R.; Kubein-Meesenburg, D.; Sadat-Khonsari, R. Initial forces generated by three types of thermoplastic appliances on an upper central incisor during tipping. *Eur. J. Orthod.* **2009**, *31*, 625–631. [[CrossRef](#)] [[PubMed](#)]
26. Luzzi, V.; Ierardo, G.; Di Carlo, G.; Saccucci, M.; Polimeni, A. Obstructive sleep apnea syndrome in the pediatric age: The role of the dentist. *Eur. Rev. Med. Pharmacol. Sci.* **2019**, *23*, 9–14. [[CrossRef](#)]
27. Ihssen, B.A.; Willmann, J.H.; Nimer, A.; Drescher, D. Effect of in vitro aging by water immersion and thermocycling on the mechanical properties of PETG aligner material. *J. Orofac. Orthop. = Fortschritte Kieferorthopadie Organ/Off. J. Dtsch. Ges. Kieferorthopadie* **2019**, *80*, 292–303. [[CrossRef](#)]
28. Lajolo, C.; Tranfa, M.; Patini, R.; Fiorino, A.; Musarra, T.; Boniello, R.; Moro, A. Clinical Evaluation of the Optical Filter for Autofluorescence Glasses for Oral Cancer Curing Light Exposed (GOCCLES((R))) in the Management of Potentially Premalignant Disorders: A Retrospective Study. *Int. J. Environ. Res. Public Health* **2022**, *19*, 5579. [[CrossRef](#)] [[PubMed](#)]
29. Sivolella, S.; Meggiorin, S.; Ferrarese, N.; Lupi, A.; Cavallin, F.; Fiorino, A.; Giraudo, C. CT-based dentulous mandibular alveolar ridge measurements as predictors of crown-to-implant ratio for short and extra short dental implants. *Sci. Rep.* **2020**, *10*, 16229. [[CrossRef](#)] [[PubMed](#)]
30. Azzi, L.; Moretto, P.; Vinci, R.; Croveri, F.; Boggio, A.; Silvestre-Rangil, J.; Tettamanti, L.; Tagliabue, A.; Passi, A. Human beta2-defensin in oral lichen planus expresses the degree of inflammation. *J. Biol. Regul. Homeost. Agents* **2017**, *31*, 77–87.
31. Azzi, L.; Rania, S.; Spadari, F.; Vinci, R.; Manfredini, M.; Croveri, F.; Boggio, A.; Tettamanti, L.; Tagliabue, A.; Silvestre-Rangil, J.; et al. Genetic correlation between rheumatoid arthritis and periodontal disease: The role of sex and IL-10. *J. Biol. Regul. Homeost. Agents* **2017**, *31*, 67–75.
32. Xiang, B.; Wang, X.; Wu, G.; Xu, Y.; Wang, M.; Yang, Y.; Wang, Q. The force effects of two types of polyethylene terephthalate glycol-modified clear aligners immersed in artificial saliva. *Sci. Rep.* **2021**, *11*, 10052. [[CrossRef](#)]

Disclaimer/Publisher’s Note: The statements, opinions and data contained in all publications are solely those of the individual author(s) and contributor(s) and not of MDPI and/or the editor(s). MDPI and/or the editor(s) disclaim responsibility for any injury to people or property resulting from any ideas, methods, instructions or products referred to in the content.